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# COMPREHENSIVE ASSESSMENT OF WEARABLE SMART TEXTILE SENSORS.

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### ABSTRACT:

This paper illustrates the comprehensive assessment and performance overview of wearable textile sensors .The manuscript depicts the challenges, state of art, merits and demerits of various wearable textile sensors developed till date. Much advancement has been made in the field of textile sensors. Wearable sensors are steadily becoming an integral part of health, fitness, biomedical, childcare and many other industries. For various applications the wearable sensor are integrated into the garments then comes the demand for the material of the sensor to be thin and flexible enough to withstand any sort of changes with the material. The evolution of wearable textile sensors depended on many factors some of them being materials being used, high performance, and miniaturization, low cost and non-invasive nature. The paper also gives a brief review about the integration technologies which make the wearable sensors easy to wear thus provide comfort with continuous monitoring. With the technology undergoing a sea change, in this field advancements are going on in wireless sensing and body sensing network.

Keywords: *Wearable's; Sensors; Textile; Smart* Sensors; Electrochemical; Gas Sensors.

### **I.INTRODUCTION:**

The field of wearable sensors in the recent years has been developing steadily with a rapid pace. The integration of nanotechnology and nanoelectronics in the field of textile has in itself brought a boom in the wearable sensor industry[1,2]. The concept behind developing wearable sensors was which could monitor the health, comfortable to wear as well as to promote the non-invasive ways which would further ease the process. With the progress the concept made its way into many fields also namely medical [3-5], for the disabled persons [6, 7], distributed sensor networks [8-10], sports and fitness industry. In this paper we would be discussing briefly about different types of wearable sensors, their integration technologies, sensor placement techniques, merits and demerits of various types of sensors, remedies of the

disadvantages and future scope. With the amount of research being done in the field till now has resulted in evolution of various kinds of wearable sensors which include electrochemical sensors, gas sensors, sweat sensors, saliva sensors, tear sensors and many more. Prior to the introduction of wearable sensors technology the health industry adopted the traditional invasive ways for health monitoring (though still quite prevalent) for e.g. blood test for a homophobic, anaemic and aged patients can prove to be quite challenging and hence non-invasive ways of analyte monitoring were developed and hence developed the concept of electrochemical sensors which include tear saliva, sweat sensors which provides a better continuous assessment of the patient's health[11-131.

There are various substitutes to blood available for analyte monitoring these days like sweat, tears, saliva etc. which show case similar relationships with the analytes present in blood like glucose, electrolytes etc.

There monitoring through the non-invasive ways will be a better option than using the invasive way of monitoring.

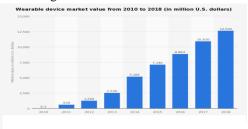


Figure1: Indicates the market share in terms of revenue of the wearable devices including sensors [62].

Now after development of the sensor the main concern should be that it should be comfortable since it is wearable and unnoticeable and hence various integration technologies which make that possible are discussed here. Then comes the need for proper placement of the sensor, indeed it is the most essential part since the signals may vary with the position of the body part and hence proper positioning is deemed necessary [14]. Automatic detection of sensor placement site may be helpful as they provide information where to place the sensor as the irregular placement of the sensor results in faulty readings .Sensor placement is deemed necessary because few sensors are site specific and will give correct readings only when placed at correct sites otherwise which would lead to corrupt readings.

The major advantage of recognising the correct sensing sites is that it will curb the error misplacement rate and will enhance the information content extracted from thus facilitating suitable data extraction.

Need of real time monitoring is increasing though these devices are limited development is going at a rapid pace. Wireless body sensors networks are widely prevalent these days in personal care systems [15].

The real time monitoring of various wearable sensors have indeed given a boost to personalised home care systems and has certainly shifted the treatment methodologies from clinical diagnostics to home based personal management.

This has certainly brought a revolution in the health industry and will certainly lower the health care costs.

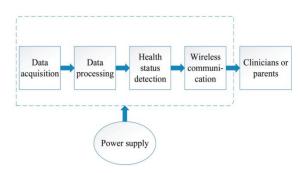


Figure 2: It indicates the basic block diagram of the functioning of the wearable sensors by using health industry as a base[63].

### II.RELATED WORK AND DISCUSSIONS:

### A. DESIGNING OF WEARABLE SENSORS:

Before starting the discussion let us first deal with the designing part of wearable sensors. As we all know that wearable sensors are a blend of electronics and textile engineering hence this in itself increases the complexity of the sensor system. Hence creating an optimum design of the sensor in itself is a herculean task because it involves integration of the electronics platform (memory, power management, receiver etc.) into the textile platform. Hence creating a wearable device which in itself is comfortable to wear and is disguisable also. The older techniques involved board level and package level integration technologies which have several demerits one of them being the finished product made using these integration technologies is that it becomes uncomfortable to wear due to the bulky nature.

Hence several new technologies were devised in order to tackle the demerits and hence creating comfortable smart wearable smart devices. Technologies to be discussed here are organic and large area electronics (OLAE) and thin film technologies [16].

# B. Organic and large area electronics platform for sensors

This mainly targets low end applications and cheap devices. Application on thin flexible plastic foils and materials used are polyesters PET and PEN.

As mentioned earlier deals with low end devices with less complexity and uses screen and inkjet printing as printing techniques[17]. Advancements are still in progress in this field to generate more complex systems through this technique.

### C. Thin film electronics platform

This technique is used for more complex high end applications and for more advanced devices .Can be termed as advanced version of OLAE technology.

Thin film electronics platform is realised by combining spin-on polyimide films with thin-film metallization.

To get the final stretchable product from the flexible foils there exists a technology named thin chip integration technology. In order to get the final finished product which is stable and can be deformed in more than one direction optimum designing techniques should be employed starting with flex foil (polyester, polyimide or other plastic foil materials), circuit made through printed circuit board techniques and then using adhesives, soldering used to assemble the components.

The chief aim of the technology is to provide comfortable wearable devices which are reliable as well as resistant to the stress which is distributed accordingly and thus fulfilling the design requirements which in turn can be used to realise any type of sensors.

# **III.TYPES OF WEARABLE SENSORS:**

## A. ELECTROCHEMICAL SENSORS:

The need of non-invasive monitoring has triggered the importance further of electrochemical sensors which include saliva, sweat. tear and skin interstitial fluid monitoring. Since all these can be used as substitutes for health monitoring instead of blood since it involves the invasive ways of checking the health status of a person which can be a tedious task in case of elderly, children and people suffering from anaemia and other blood diseases. Hence the sensors are mentioned below:

# **B.** TEAR SENSORS:

Tears are composed of lipids, electrolytes, metabolites .There is a relation between the glucose composition of blood and tears [18] hence can be used as non-invasive monitoring for the diabetes patients and thus aiding in clinical diagnostics.

The initial ocular sensors were based on strip based flexible sensors in them the electrodes were fabricated with the stretchable platforms [19-24].It used low cost printing technology in order to obtain the finished sensor product [25].

Utilisation of strip based sensors was done in monitoring keratoconjunctivitissicca [19], transcutaneous oxygen [20], and glucose [21– 25].The more advanced version for ocular sensor developed was soft contact lens with a blend of wireless electronics [26-28].In the initial stages of the work it was hand wired later on integration of wireless electronics happened for data storage and charging purpose, the work was again modified to reduce interference [26, 27]

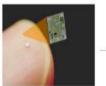
In the recent developments Novio sense glucose sensors being developed in Netherlands for glucose monitoring with the placement of the sensor being within eyelids [29].Real time monitoring with wireless platform still remains a challenge in the industry.

# DISADVANTGES/CHALLENGES OF TEAR SENSORS:

Evaporation of the tear sample may take place before the analysis which may affect the concentration of analytes and thus hampering the final results of the diagnosis. Since eye is one of the most delicate organs of the body utmost care needs to be taken while collecting the sample.

The sensors uses flexible and stretchable materials but still are hard which may cause irritation in eyes which may trigger eye to release reflex tears which may cause recording of false readings thus altering the diagnosis data.

While monitoring the glucose levels in an eye prolonged eye closure, exposure to vapours any sort of mechanical disturbance may cause altering of glucose levels in an eye [30].Real time monitoring using wireless platform still remains a challenge to be addressed at a larger scale.







Close-up of wireless chip Chip, sensor and antenna mounted Figure 3: Tear based sensors[64].

Electronics ring embedded in contact lens

# C. SWEAT BASED SENSORS:

Sweat is composed of water (99%) and electrolytes, urea, pyruvate and lactate [31, 32]. Among the sweat the concentration of sodium (Na+) is highest among all the electrolytes [33].

The PH level of sweat and the concentration of sodium level are inter related, the PH and sodium level are directly proportional to each other.PH amount gives a brief idea about the hydration and dehydration levels of the body which can be utilised to monitor these levels in the body of an athlete.

As the PH level as shown is related to the health of a person and if it changes this promotes various kinds diseases [34]. The sweat is a perfect medium which carries information useful for various medical pathologies in general. Sweat is used to monitor electrolyte imbalance[39], physical stress[40],bone loss[41],persons mineral intoxication level[42],drug abuse[43], osteoporosis[44]. Real time sweat while monitoring using calorimetric and electrochemical sensors has been a major achievement in the given field [35, 36].

The integration of sensors into textile is feasible; sol gel process is used to form a fully functionalised fabric. Sol gel technology has various organic and inorganic additives related to it. The major advantage of sol gel technology is thermal and mechanical robustness .Sol gel technology is basically used to obtain the PH performance. Major disadvantage being long response time keeping this in mind caldra et.al [37optical monitoring] proposed the use of mesoporous thin film prepared by sol gel chemistry and low temperature block co polymer extraction this can work quite efficiently as a PH sensor and it also improves the response time.

Sweat was also used as a medium to test ethanol using a device based on an amperometric biosensor characterized by a graphite electrode with embedded alcohol oxidase, horseradish peroxidise and ferrocene, in the presence of a working solution (0.05 M, pH7.4), separated by a PTFE membrane from the contacting skin, used to detect and monitor ethanol within 5 mins thus making these sensors multitasking operators [38].

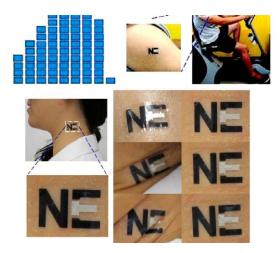


Figure 4: Indicates the stretchable tattoo based sensor[65].

The non-invasive sweat monitoring for monitoring sweat may be of two types:

Fabric/flexible plastic based [45]; Epidermal based sensors [46]

# D. FABRIC/FLEXIBLE PLASTIC BASED:

Fabric used to development of sensor due to contact with skin. They provide large surface area and thus integration of electronics in that area. Fabrics such as wool, cotton and nylon etc have physical and chemical properties associated with them and thus facilitate the integration of chemical sensor with it.

The textile should be inert in nature as being inert in nature is advantageous in a situation where there shall be no effect on the chemical behaviour of the analyte. Thus there is need of complete coordination between sensor and textile so as to operate smoothly.

Sensors show response when in direct contact with the skin.Eg being sensor installed on the waistband of the undergarments which monitors the sweat [47] another example being PH sensor on bandage for keeping a check on the wound [48].Main advantage of printed textile sensor is that they are bendable and stretchable platforms thus providing themselves flexibility of placements.

When contact with electrode surface and bio fluid takes place confirms smooth functioning of wearable sensors, since skin contact is quite limited hence this is quite challenging for the fabric based system and may be termed as one of the demerits of these systems.

This triggers the need of epidermal electrochemical sensors.

### E. EPIDERMAL BASED SENSORS:

Analyte monitoring over the skin by using epidermal electrochemical sensors. Electrodes printed directly on human epidermis [49].Process involves wetting of customized stamps with conductive ink then comes printing of electrode design on the skin. This was further resolved by using tattoo based electrochemical sensors [50].Tattoo based sensors are resistant to such deformation by using carbon fibres. Electrical energy harnessed from human sweat known has epidermal bio fuel cell [51].

Sweat based sensors measuring PH has certain advantages:

Has high signal to noise ratio, longer life time, they are reversible, fast response, durable, cheap, comparatively safer than ocular based sensors.

Some of the disadvantages mainly are as follows: They have a poor selectivity and long term instability. As the physical activity of the person increases there is a deformation in the sensor.



Figure 5: Sensor present at the strip of the underwear used for sweat monitoring[65].

### F. SALIVA BASED SENSORS:

Saliva is another substitute and the most effective non-invasive monitoring technique available .Saliva also has few of its components same as that of the blood according to the research it has successfully been used to monitor several neurological parameters [52].Major advantages of saliva is its easy availability, relation of its analyte concentration with blood, certain initial treatment procedures before using it for diagnosis are less.

The developments that has been accomplished in the field of saliva based sensors are

Because of its vicinity with the teeth it is widely used to monitor fluoride levels in a teeth [53].Disadvantage of the above technique is it's difficult to provide each tooth with sensor. In future need for real time monitoring with the integration of wireless electronics in this field is also the need of the hour.

Recent development of the dental tattoo with wireless electronics integrated used to monitor bacteria in the mouth was a real success [54]

Involvement of wireless electronics with the sensors generate many advantages few of them being they have less response time which makes the functioning faster, they are highly specific about the test, they can detect a single molecule also if needed.

The monitoring of PH level and glucose level to test the diabetes by using saliva as a medium is still very popular.PH level is also used for GERD testing which otherwise is tested by using invasive oesophagus surgery[55].

Saliva is also used for testosterone monitoring, the process is carried out is as follows the saliva is first treated with charcoal then by using the process of centrifugal the charcoal was removed this was done because the analyte corresponding to it was in lesser concentration in saliva so in order to be specific this was done. This later facilitates in the real time monitoring of the system and the results were displayed within 10 minutes of monitoring the whole system [56].

#### G. TEXTILE GAS SENSORS:

The textile gas sensors are a somewhat refined version of old wearable sensor concepts. Pressure

and temperature sensors are quite feasible to operate as compared to gas sensors.

Disadvantage of gas sensors being they possess complex structure, the exposure to environmental conditions of the gas sensitive elements in a sensor is the major drawback of the sensor. Since if used as a air filter then exposure to external environmental conditions may lead to malfunctioning of the air filter which may prove to be fatal.

Thus the above reasons pose a difficulty in realising gas sensors which have their utility in disposable air filters and other clinical diagnosis garments i.e., basically utility in health sector itself[57].

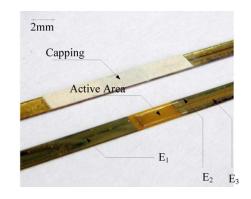


Figure 6: Shows gas sensors with and without capping layer [66].

Recent developments in the gas sensor have been: General long strip like designed sensor has an acrylic co polymer layer which aids and shields against the environmental conditions which has been the main cause of concern while designing gas sensor. Gas sensing is done by planar capacitor and resistor. Other less bulky light weight sensors using plastic foils as a platform were also reported [58, 59].

Fabrication process is simple and is quite cheap.

Necessary requirements for the smooth functioning of the sensor are: at first the active area of the sensor should be isolated from the external environmental conditions so that it could be saved from the malfunctioning.

Another important factor being that repeated bending test should be done so as to test the mechanical robustness it's so that future performance of the sensor can be judged accordingly.

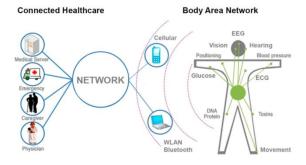


Figure 7: Shows the interconnection between body and various wearable platforms [67].

# **IV.CONCLUSION AND FUTURE TRENDS:**

The field of nanotechnology has developed with a rapid pace hence increasing its applications in various fields. Wearable sensors are one such kind which involves blend of physics, chemistry, electrical and textile engineering with a special integration of nanotechnology and material sciences. Wearable sensors have now established their utility in many fields and will continue to grow with the amount of research opportunities growing in this field. More widely accepted in the field of healthcare is expanding its area of application with time. Wearable sensors with large area are generally easy to realise whereas when miniaturization takes places and the area of interest shrinks then several variations are needed to be made in order to develop a sensor which is best suited with the appropriate changes in area. With the development of wearable sensors it also encounters several challenges as the work progresses. First problem is faced while printing as the dimension of the printed work is quite larger than the actual dimension [60] which then causes the problem of irregular shape. At first the wearable sensors were aimed at only producing disposable sensors but as the time progressed washable wearable sensors have slowly started dominating the markets because of their advantage of reusability but with the advantages they also address few challenges the biggest of them being maintaining that same strength, flexibility even after washing and the internal functioning and circuitry is saved from all types of external agents which may hamper the productivity and performance of the sensors. Now while discussing about the external agents we can install temperature sensors in the sensors as the environmental changes

also affects the performance of the sensors. Since electronic circuitry is also involved complete encapsulation of the sensor is required of that area against any sort of aqueous solution so as to prevent malfunctioning. As the wearable sensors finds their application in health care industry the nanomaterials used while designing of the sensors should be checked of their toxicity levels which in case if not happens then prove to be fatal though it is a non-invasive method but still even direct contact with the skin of the toxic materials may be harmful. But they prove to be a merit over the invasive techniques as they may cause infections. Now after ensuring the safety of the user the sensors safety is also necessary proper covering should be there in order to save it from any sort of virus, fungal and bacterial attack which ensures correct data reception without any fail. Bending test should be conducted of every sensor so that durability of the sensor can be known. Ideal characteristics of an wearable sensor is that: low cost, low power consumption, mechanically roboust, can perform complex tasks, minimizing size &maximizing comfort , highly efficient, showcases long term stability, biocompatibility, user sensor, selectivity, durable, supports independent wireless platform. These are the characteristics desired in a wearable sensor. In recent years a lot has been to done to achieve these characteristics by various methods and techniques. In order to develop sensor in this field there has to be some sort of coordination between the research universities and the manufacturing companies so as to promote the idea and finally realise it because these two factors go hand in hand. Real time monitoring system development has certainly become the need of the hour where several devices are solely focused to monitor the actual situation in which the person is gives accurate results within a small response time. This brought the health diagnosis to your door step. A lot of work still needs to be in integrating wireless platform as it not only decreases the response time but also makes the sensor more efficient but with this the wearable sensor becomes more complex because of integration of wireless modules. Challenges go hand in hand with the new inventions thus a lot needs to be done in this field. Also this is quite popular with the health industry for diagnosis and medical checkups whereas shifting the focus and using it in sports and different other fields would be an added advantage to it.

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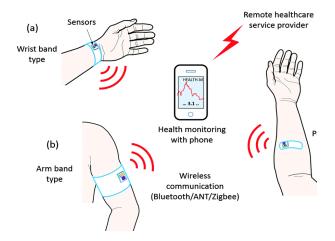
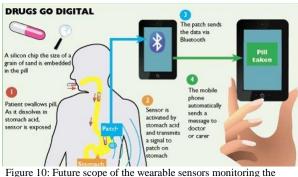


Figure 8: Real time monitoring through wireless platform [68].



Figure 9: Apple watch a revolution in the wearable electronics market[69].



operations inside the body [70].

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### **References:**

[1] B. Mahltig, T. Textor, Nanosols and Textiles, 1st ed., World Scientific, London, 2008.

[2] E. Guido, J. Alongi, C. Colleoni, A. Di Blasio, F. Carosio, M. Verelst, G. Malucelli,G. Rosace, Thermal stability and flame retardancy of polyester fabrics sol-gel treated in the presence of boehmite nanoparticles, Polym. Degrad. Stabil. 98(2013) 1609–1616.

[3] A. Pantelopoulos, N.G. Bourbakis, A survey on wearable sensor-based systems for health monitoring and prognosis, IEEE Transactions on Systems, Man, and Cybernetics, Part C: Applications and Reviews 40 (1) (2010) 1–12

[4] S. Pasche, S. Angeloni, R. Ischer, M. Liley, J. Lupranoe, G. Voirinf, Wearable biosensors for monitoring wound healing, Advances in Science and Technology 57 (2008) 80–87.

[5] R. Jafari, R. Bajcsy, S. Glaser, B. Gnade, M. Sgroi, S. Sastry, Platform design for health-care monitoring applications, in: HCMDSS, vol. 07, 2007, pp. 1–7.

[6] M. Bächlin, M. Plotnik, D. Roggen, I. Meidan, J.M. Hausdorff, N. Giladi, G. Tröster, Wearable assistant for Parkinson's disease patients with the freezing of gait symptom, IEEE Transactions on Information Technology in Biomedicine 14 (2) (2010) 436–446.

[7] T. Giorgino, S. Quaglini, F. Lorassi, D. De Rossi, Experiments in the detection of upper limb posture through kinestetic strain sensors, International Workshop on Wearable and Implantable Body Sensor Networks (2006) 4–12.

[8] C. Lauterbach, R. Glaser, D. Savio, Markus Schnell, W. Weber, S. Kornely, A. Stöhr, A self-organizing and fault-tolerant wired peer-to-peer sensor network for textile applications, Lecture Notes in Computer Science 3464 (2005) 256–266.

[9] D. Graumann, G. Rama, M. Quirk, B. Sawyer, J. Chong, M. Jones, T. Martin, Large surface area electronic textiles for ubiquitous computing: a system approach, in: Fourth Annual International Conference on International Journal of Advanced Information Science and Technology (IJAIST)ISSN: 2319:2682Vol.5, No.1, January 2016DOI:10.15693/ijaist/2016.v5i1.30-39

Mobile and Ubiquitous Systems: Networking and Services, 2007.

[10] I. Locher, T. Kirstein, G. Tröster, Temperature profile estimation with smart textiles, in: Proceedings of the 1st International Conference on Ambient and Systems, 2005, pp. 1–8.

[11]Windmiller, J.R. and Wang, J. (2013) Wearable electrochemical sensors and biosensors: a review. Electro analysis 25, 29–46

[12] Kim, D.H. et al. (2012) Inorganic semiconductor nanomaterials for flexible and stretchable bio-integrated electronics. NPG Asia Mater. 4, e15

[13] Hammock, M.L. et al. (2013) 25th anniversary article: the evolution of electronic skin (e-skin): a brief history, design considerations, and recent progress. Adv. Mat. 25, 5997–6038

[14] K. Kunze, P. Lukowicz, Sensor placement variations in wearable activity recognition, IEEE Pervasive Comput. 13 (2014) 32–41.

[15] Y. Hao, R. Foster, Wireless body sensor networks for health-monitoring applications, Physiol. Meas. 29 (2008) R27.

[16] Jeroen van den Brand , Margreet de Kok , Marc Koetse , Maarten Cauwe , Rik Verplancke ,Frederick Bossuyt , Michael Jablonski , Jan Vanfleteren, Flexible and stretchable electronics for wearable health devices, Solid-State Electronics 113 (2015) 116–120.

[17] VanOsch THJ, Perelaer J, de Laat AWM, Schubert US. Inkjet printing of narrow conductive tracks on untreated polymeric substrates. Adv Mater2008; 20:343–5.

[18]Yan, Q. et al. (2011) Measurement of tear glucose levels with amperometric glucose biosensor/capillary tube configuration. Anal. Chem. 83, 8341–8346

[19] Ogasawara, K. et al. (1996) Electrical conductivity of tear fluid in healthy persons and keratoconjunctivitis sicca patients measured by a flexible conductimetric sensor. Graefes Arch. Clin. Exp. Ophthalmol. 234, 542–546

[20] Iguchi, S. et al. (2005): A Wearable oxygen sensor for transcutaneous blood gas monitoring at the conjunctiva. Sens. Actuat. B 108, 733–737

[21] Kudo, H. et al. (2006) a flexible and wearable glucose sensor based on functional polymers with Soft-MEMS techniques. Biosens. Bioelectron. 22, 558–562 [23] Iguchi, S. et al. (2007) A flexible and wearable biosensor for tear glucose measurement. Biomed. Micro devices 9, 603–609

[24]Chu, M.X. et al. (2011) biomedical soft contact-lens sensor for in situ ocular bio monitoring of tear contents. Biomed. Micro devices 13, 603–611

[25] Kagie, A. et al. (2008) Flexible rolled thick-film miniaturized flow-cell for minimally invasive amperometric sensing. Electro analysis 20, 1610–1614

[26] Yao, H. et al. (2011) A contact lens with embedded sensor for monitoring tear glucose level. Biosens. Bioelectron. 26, 3290–3296

[27] Liao, Y.T. et al. (2012) A 3–mW CMOS glucose sensor for wireless contact-lens tear glucose monitoring. IEEE J. Solid State Circuits 47, 335–344

[28] Yao, H. et al. (2012) A contact lens with integrated telecommunication circuit and sensors for wireless and continuous tear glucose monitoring. J. Micromech. Microeng. 22, 075007–075016

[29] Amay J. Bandodkar and Joseph Wang, Non-invasive wearable electrochemical sensors: a review, Trends in Biotechnology July 2014, Vol. 32, No. 7.

[30] Daum, K.M. and Hill, R.M. (1984) Human tears: glucose instabilities. Acta Ophthalmol. 62, 530–553

[31] A. Mena-Bravo, M.D. Luque de Castro, Sweat: a sample with limited present applications and promising future in metabolomics, J. Pharm. Biomed. Anal.90 (2014) 139–147

[32] C.J. Harvey, R.F. LeBouf, A.B. Stefaniak, Formulation and stability of a novel artificial human sweat under conditions of storage and use, Toxicol. In Vitro24 (2010) 1790–1796.

[33] M.J. Patterson, S.D.R. Galloway, M.A. Nimmo, Variations in regional sweat composition in normal human males, Exp. Physiol. 85 (2000) 869–875.

[34] V.F. Curto, S. Coyle, R. Byrne, N. Angelov, D. Diamond, F. Benito-Lopez, Concept and development of an autonomous wearable micro-fluidic platformfor real time pH sweat analysis, Sens. Actuators B 175 (2012) 263–270.

[35] S. Coyle, D. Morris, K.-T. Lau, D. Diamond, F. Di Francesco, N. Taccini, M.G.Trivella, D. Costanzo, P. Salvo, J.-A. Porchet, J. Luprano, Textile sensors to measure sweat pH and sweat-rate during exercise, in: 3rd International Conference on Pervasive Computing International Journal of Advanced Information Science and Technology (IJAIST) ISSN: 2319:2682 Vol.5, No.1, January 2016 DOI:10.15693/ijaist/2016.v5i1.30-39

Technologies for Healthcare, London, UK,April 1–3, 2009, ISBN: 978-963-9799-42-4.

[36] D. Morris, S. Coyle, Y. Wu, K.T. Lau, G. Wallace, D. Diamond, Bio-sensing textilebased patch with integrated optical detection system for sweat monitoring, Sens. Actuators B: Chem. 139 (2009) 231–236.

[37] Michele Caldara, Claudio Colleoni, Emanuela Guido, Valerio Re, Giuseppe Rosace, Optical monitoring of sweat pH by a textile fabric wearable sensorbased on covalently bondedlitmus-3glycidoxypropyltrimethoxysilane coating, Sensors and Actuators B 222 (2016) 213–220.

[38] M. Gamella, S. Campuzano, J. Manso, G. Rivera, F. López-Colino, A. Reviejo, et al., A novel non-invasive electrochemical bio sensing device for in situ determination of the alcohol content in blood by monitoring ethanol in sweat, Anal.Chim. Acta 806 (2014) 1–7.

[39] Bergeron, M.F. (2003) Heat cramps: fluid and electrolyte challenges during tennis in the heat. J. Sci. Med. Sport 6, 19–27

[40] Pilardeau, P.A. et al. (1979) Secretion of eccrine sweat glands during exercise. Br. J. Sports Med. 13, 118–121

[41] Klesges, R.C. et al. (1996) Changes in bone mineral content in male athletes mechanisms of action and intervention effects. J. Am. Med. Assoc. 276, 226–230

[42] Gamella, M. et al. (2014) A novel non-invasive electrochemical bio sensing device for in situ determination of the alcohol content in blood by monitoring ethanol in sweat. Anal. Chim. Acta 806, 1–7

[43] Burns, M. and Baselt, C. (1995) Monitoring drug use with a sweat patch: an experiment with cocaine. J. Anal. Toxicol. 19, 41–48

[44] Heaney, R.P. (1992) Calcium in the prevention and treatment of osteoporosis. J. Int. Med. 231, 169–180

[45] Windmiller, J.R. and Wang, J. (2013) Wearable electrochemical sensors and biosensors: a review. Electroanalysis 25, 29–46

[46] Windmiller, J.R. et al. (2012) electrochemical sensing based on printable temporary transfer tattoos. Chem. Commun. 48, 6794–6796

[47] Yang, Y.L. et al. (2010) Thick-film textile-based amperometric sensors and biosensors. Analyst 135, 1230–1234

[48]Guinovart, T. et al. (2014) Bandage-based wearable potentiometric sensor for monitoring wound ph. Electroanalysis http://dx.doi.org/ 10.1002/elan.201300558

[49] Windmiller, J.R. et al. (2012) Stamp transfer electrodes for electrochemical sensing on non-planar and oversized surfaces. Analyst 137, 1570–1575

[50] Windmiller, J.R. et al. (2012) electrochemical sensing based on printable temporary transfer tattoos. Chem. Commun. 48, 6794–6796

[51] Jia, W. et al. (2013) epidermal biofuel cells: energy harvesting from human perspiration. Angew. Chem. Int. Ed. Engl. 52, 7233–7236

[52] Aguirre, A. et al. (1993) Sialochemistry: a diagnostic tool? Crit. Rev. Oral Biol. Med. 4, 343–350

[53] Graf, H. and Mu<sup>--</sup> hlemann, H.R. (1969) Oral telemetry of fluoride ion activity. Arch. Oral Biol. 14, 259–263

[54] Mannoor, M.S. et al. (2012) Graphene-based wireless bacteria detection on tooth enamel. Nat. Commun. 3, 763–770

[55] M.B. Lerner, N. Kybert, R. Mendoza, R. Villechenon, M.A.B. Lopez, A.C. Johnson, Scalable, non-invasive glucose sensor based on boronic acid functionalized carbon nanotube transistors, Appl. Phys. Lett. 102 (2013) 183113.

[56] J.S. Mitchell, T.E. Lowe, Ultrasensitive detection of testosterone using conjugate linker technology in a nanoparticle-enhanced surface plasmon res-onance biosensor, Biosens. Bioelectron. 24 (2009) 2177–2183.

[57] P. Ghosh, Fiber Science and Technology, First ed., Tata McGraw Hill, New Delhi, 2004.

[58]A. Oprea, J. Courbat, N. Bârsan, D. Briand, N.F. deRooij, U. Weimar, Temperature,humidity and gas sensors integrated on plastic foil for low power applications, Sensors and Actuators B-Chemical 140 (2009) 227–232.

[59] J. Courbat, D. Briand, N.F. deRooij, Foil level packaging of a chemical gas sensor, Journal of Micromechanics and Micro engineering 20 (2010) 055026.

[60] F. Molina-Lopez, D. Briand, N.F. de Rooij, All additive inkjet printed humidity sensors on plastic substrate, Sensors and Actuators B: Chemical 166–167 (2012) 212–222.

International Journal of Advanced Information Science and Technology (IJAIST)ISSN: 2319:2682Vol.5, No.1, January 2016DOI:10.15693/ijaist/2016.v5i1.30-39

[61] C. Ataman, T. Kinkeldei, G. Mattana, A. Vásquez Quintero, F. Molina-Lopez, J. Courbat,K. Cherenack, D. Briand, G. Tröster, N.F. de Rooij, A robust platform for textile integrated gas sensors, Sensors and Actuators B 177 (2013) 1053– 1061.

[62]http://www.intellectsoft.net/community/development/ wearable-apps-where-we-are-where-were-going.

 [63] Zhihua Zhu, Tao Liu , Guangyi Li, Tong Li and Yoshio Inoue, Wearable Sensor Systems for Infants, Sensors 2015, 15(2), 3721-3749; doi:<u>10.3390/s150203721</u>
[64]<u>http://www.dailytech.com/Google+Signs+Controversi</u> al+Deal+With+Pharmaceutical+Giant+Novartis/article362

[65] Jia, W. et al. (2013) electrochemical tattoo biosensors for real-time non-invasive lactate monitoring in human perspiration. Anal. Chem. 85, 6553–6560.

17.htm

[66]<u>http://www.intellectsoft.net/community/development/</u> wearable-apps-where-we-are-where-were-going.

[67]Stepan Gorgutsa, Victor Bélanger-Garnier, Bora Ung, Jeff Viens, Benoit Gosselin, Sophie LA Rochelle and Younes Messaddeq,Novel Wireless-Communicating Textiles Made from Multi-Material and Minimally-Invasive Fibers,Sensors 2014, 14(10), 19260-19274; doi:10.3390/s141019260.

[68] Je-Hyeong Bahk, Haiyu Fang, Kazuaki Yazawa and Ali Shakouri ,Flexible thermoelectric materials and device optimization for wearable energy harvesting,J. Mater. Chem. C, 2015,3, 10362-10374 DOI: 10.1039/C5TC01644D

[69] http://www.notey.com/blogs/jawbone-up.

[70]https://bocaratonconciergedoctor.wordpress.com/tag/ ingestible-sensors/ and robotics, antenna and radio frequency, sensors and control systems



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